



中国汽车工程研究院股份有限公司  
China Automotive Engineering Research Institute Co., Ltd.

# Research on Reclined Occupant Safety in Frontal Impact and Draft Test and Assessment Protocol

James C. Cheng<sup>1</sup>, Yu Liu<sup>1</sup>, Jing Fei<sup>1</sup>, Peifeng Wang<sup>1</sup>, Jie Jiang<sup>1</sup>, Zhonghao Bai<sup>2</sup>, Qiang Wang<sup>2</sup>, Xiaoting Yang<sup>2</sup>, Kui Li<sup>3</sup>, Guojie Wang<sup>1</sup>, Kuo Cheng<sup>1</sup>

*1 China Automotive Engineering Research Institute Co., Ltd 2 Hunan University 3 Chongqing Medical University*

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**Speaker: Peifeng Wang**

**Position & Department:** Safety Test and Assessment System Research Engineer, Automotive Safety Technology Center, CAERI

**email: [wangpeifeng@caeri.com.cn](mailto:wangpeifeng@caeri.com.cn)**

**2025/05/21**



# Organization and Team



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Enterprise



Research  
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Listed Company

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Automotive Safety Technology Center

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Accident

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Test

Simulation



中国保险汽车安全指数  
CHINA INSURANCE AUTOMOTIVE SAFETY INDEX



Professional and Advanced  
Technical Services



Technological Support for High-quality and  
Sustainable Development



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# Research Background

## High Market Penetration Rate and Popular with Consumer



- 87.5% Penetration Rate (28/32 OEMs)  
\*Source: CAERI Investigation 2023-2024

## Higher mortality Risk and Injury Severity in Accidents

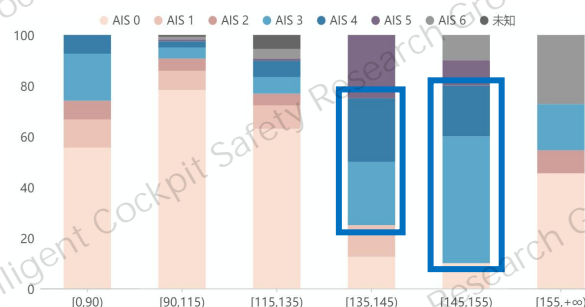
**Table 4** Mortality Risk With Full or Partial Recline, Compared With Occupants in the Upright Position

Seat Position	Adjusted Odds Ratio for Mortality	95% CI
Partial reclined	1.15	1.05-1.26
Fully reclined	1.77	1.09-2.88

Adjusted for age, sex, height, weight, seatbelt use.

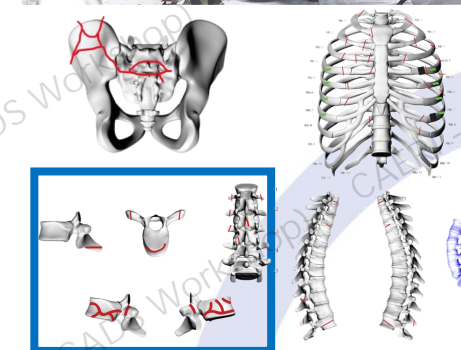
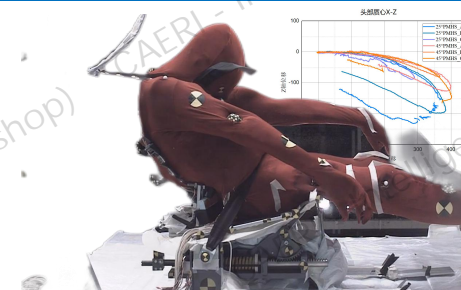
- Higher mortality of reclined occupants

\*Source: NASS/CDS N=90412 [1]



- Higher proportion of AIS 3+ injuries  
\*Source: FASS N=3270

## New Injuries and Higher Injury Severity in Tests

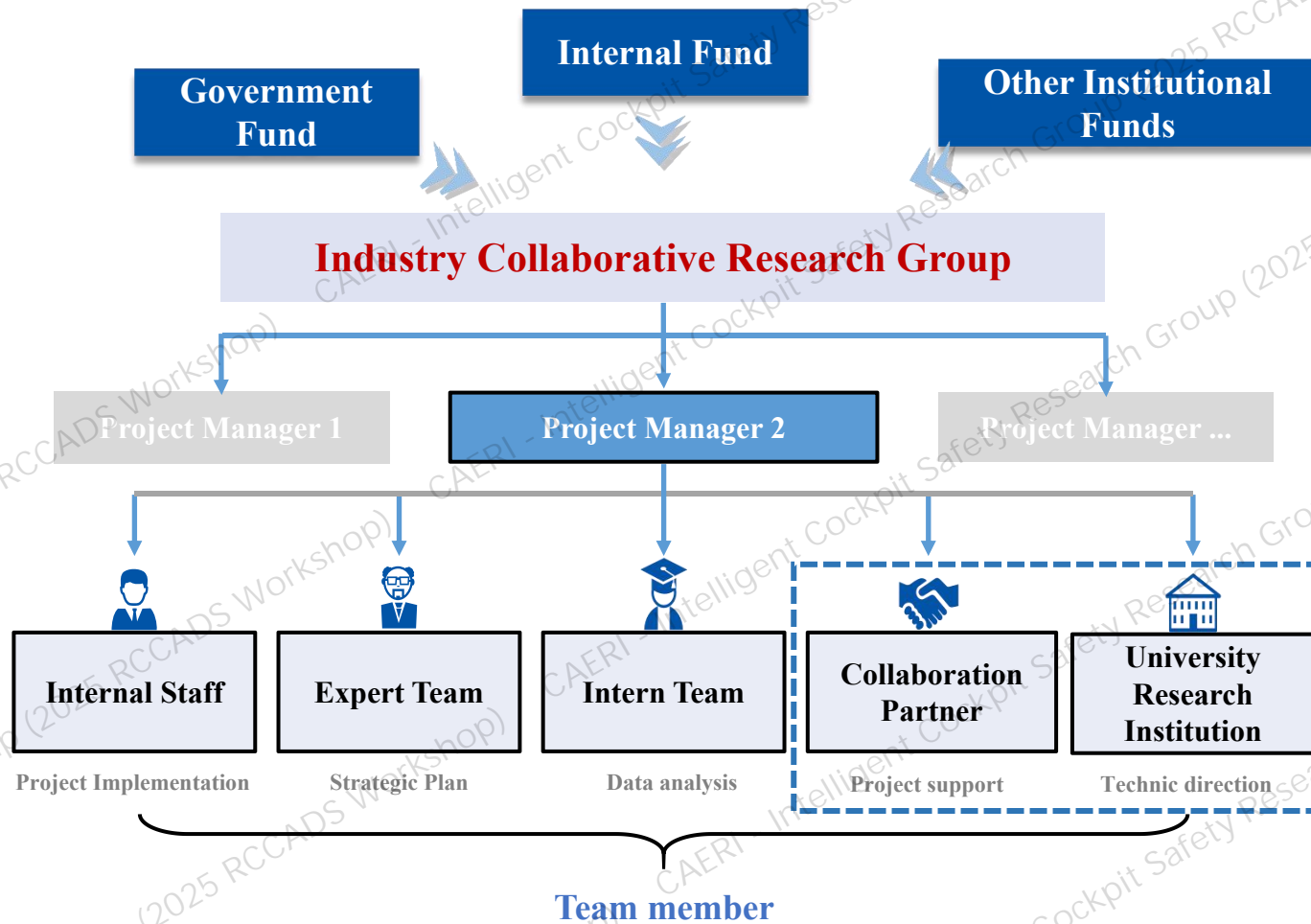


- Submarining, Iliac wing, sternum, ribs and spine fractures

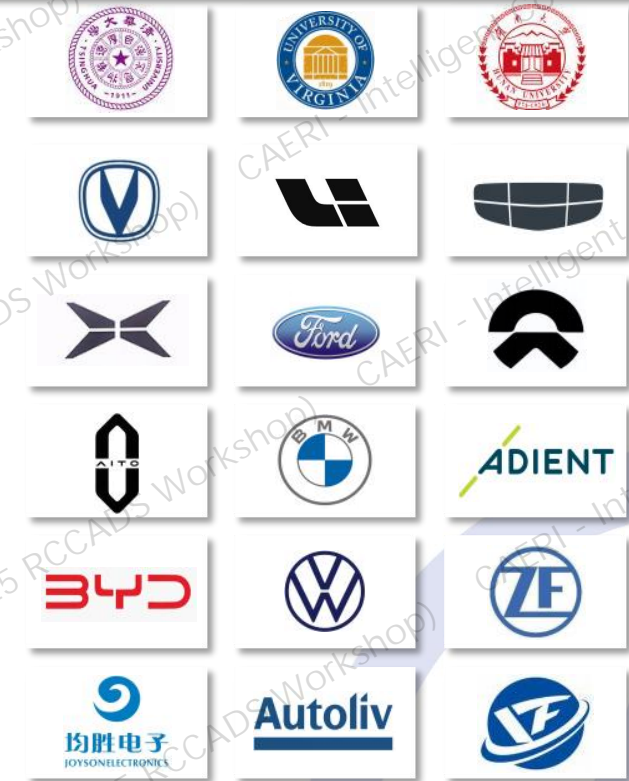
\*Source: UMTRI & UVA PMHS Tests Reports

There is **no** test and assessment protocol to ensure **reclined occupants safety** in collisions.





## Intelligent Cockpit Safety Research Group



More are coming in ...





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Background

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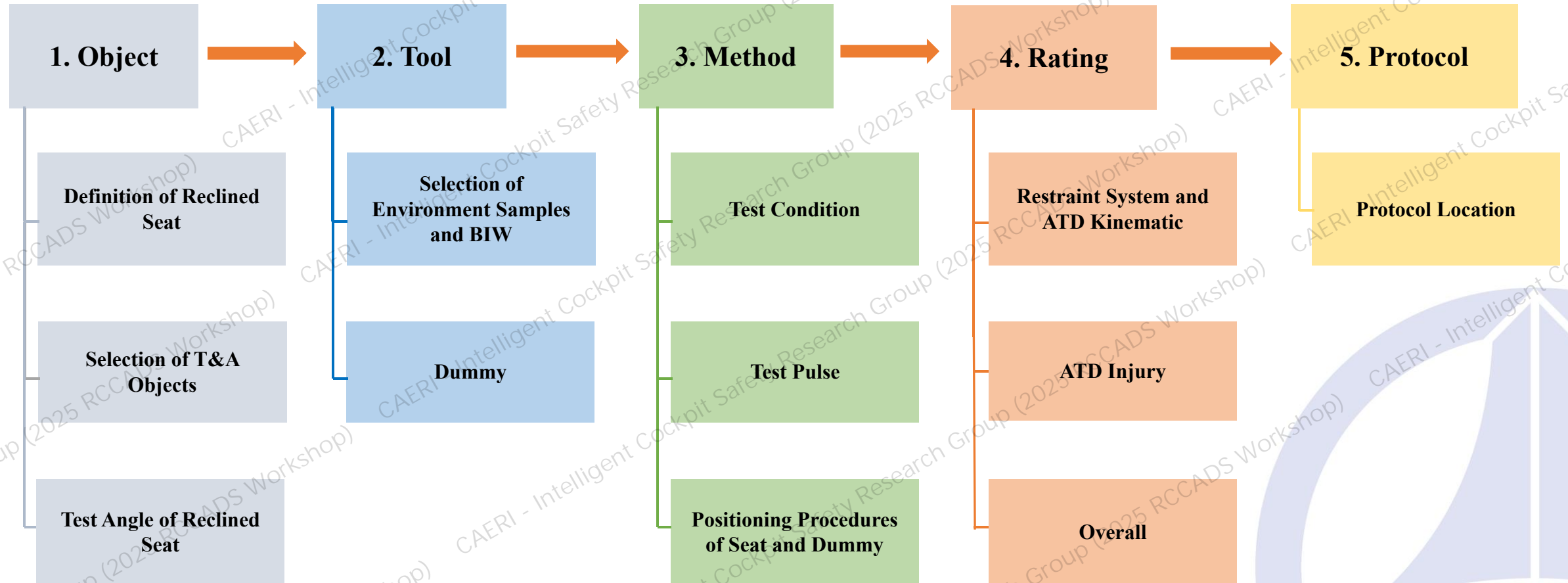
Research and Draft Protocol

3

Future Work



# Frame



## ■ Definition of Reclined Seat

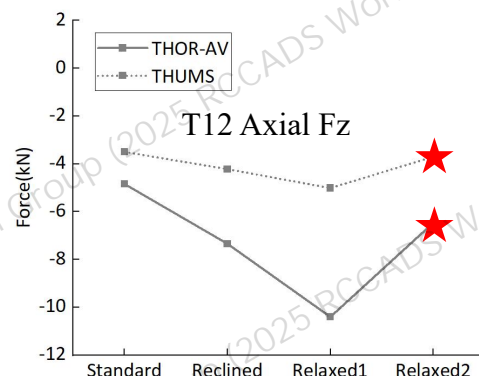
- Automotive reclined seats refer to automotive seats that **can adjust the angle** of components including the **seat cushion**, **seat back**, and **leg/foot support** to make the occupants' posture different from the traditional sitting posture.
- After adjustment, the seat cushion angle is greater than **10°** and the torso angle is greater than **35°** (measured by HPM-II).

## ■ Selection of T&A Objects

- Reclined seats which are forbidden during driving are not within the scope of the protocol, but **reports** must be provided.

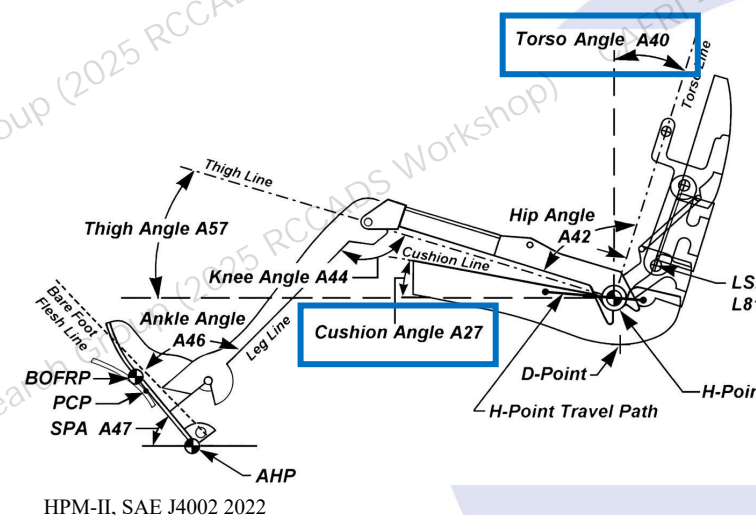
## ■ Test Angle of Reclined Seat

- Prioritize testing according to the **OEM-recommended reclining angles**. If not available, test according to the **maximum** seat back reclining angle.



Posture	Torso Angle	Cushion Angle	Leg Support Angle
Upright	25°	15°	\
Partial Reclined	45°	25°	\
Fully Reclined 1	56°	15°	40°
Fully Reclined 2	65°	30°	30°

★ submarining





## ■ Selection of Environment Samples and BIW

- If the reclined seat is in the front row, BIW and interior components such as the IP panel need to be configured. If it is in the rear row, the front-row seats are required, and the others are optional.

## ■ Dummy



### Selection Principles

#### • Biofidelity

- Published paper, presentations and other reports or public materials
- PMHS corridor and ATD responses

#### • Test Execution

- Repeatability
- Durability

#### • Price

- Price and Service

#### • Consistent with Global Protocols

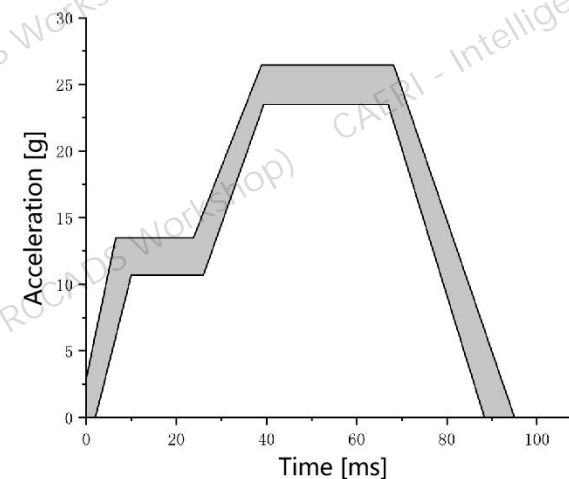
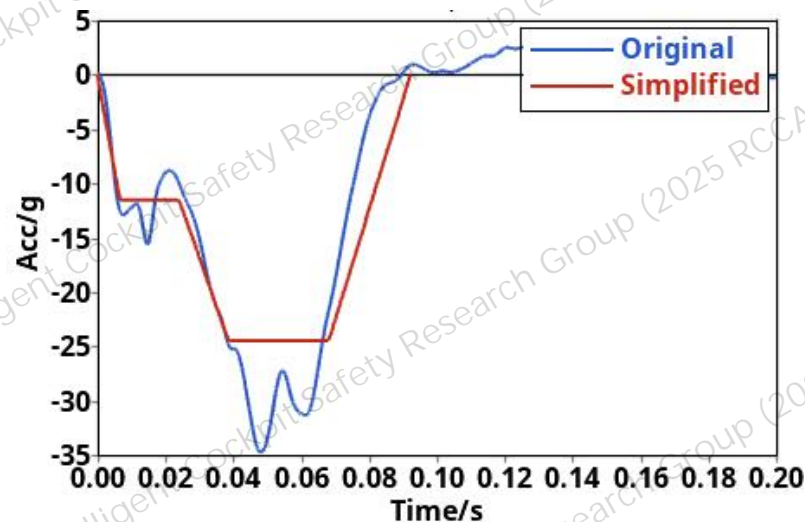
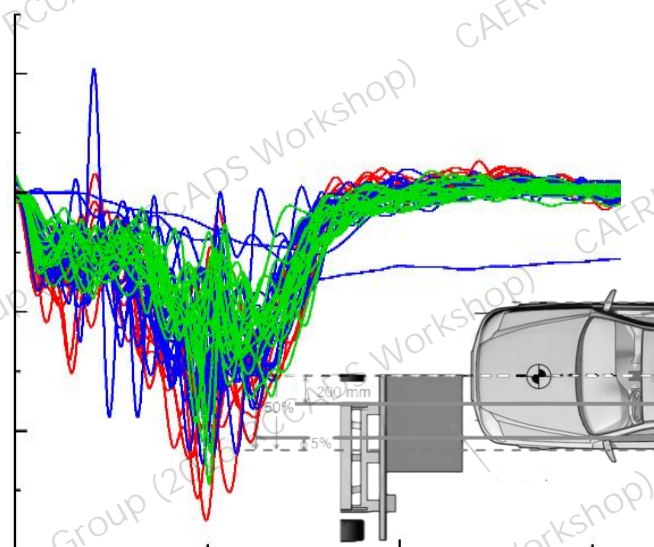
- Consistent with EuroNCAP, IIHS, etc.

#### • Others (IRCs, FE model, etc.)

- Available injury risk curves
- Available and validated FE model

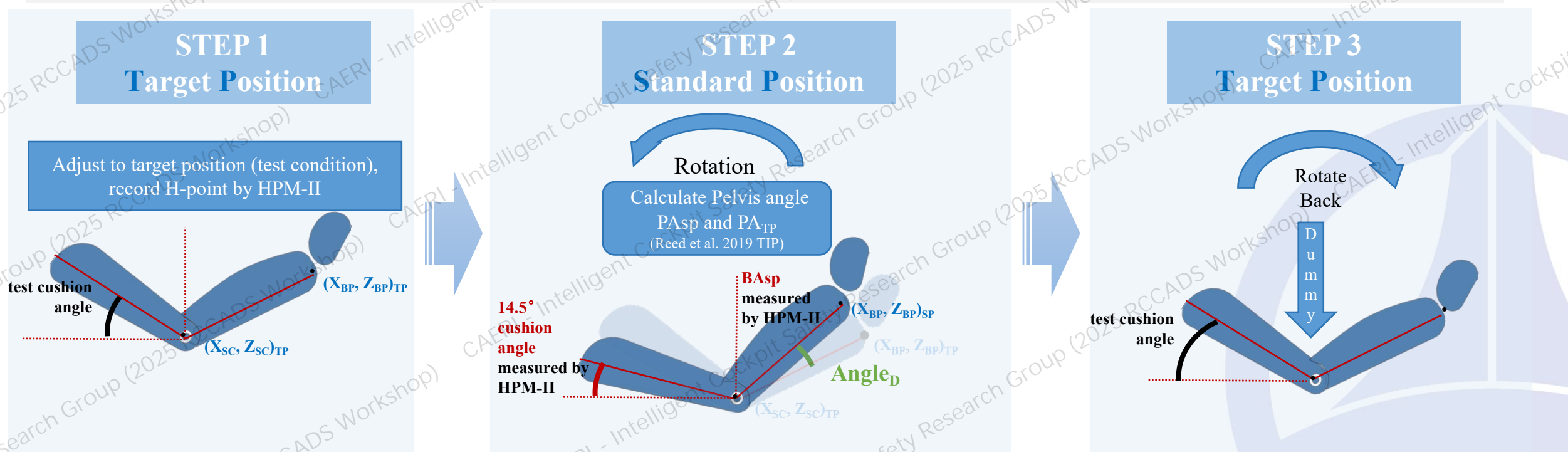
## ■ Test Pulse

- Extract the characteristics of the vehicle acceleration curves from over 50 tests of **moderate-offset frontal collisions between two vehicles with equal mass and stiffness**. Simplify them into a double - trapezoidal pulse to serve as the standard input and corridor for testing.



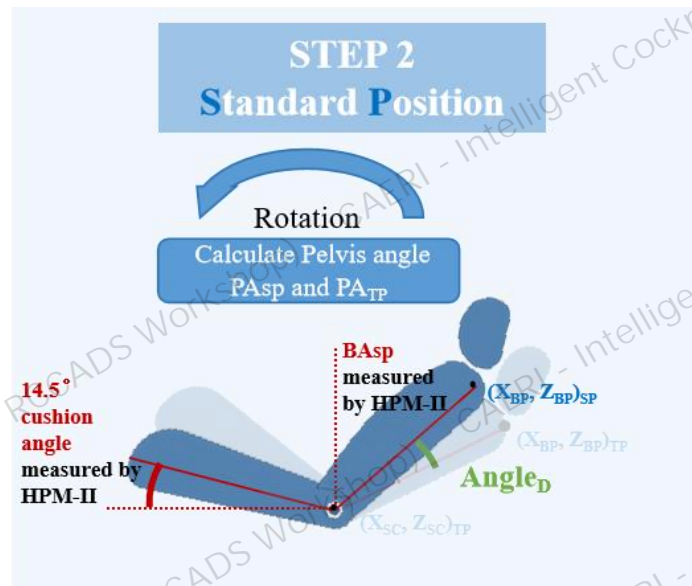
## ■ Adjustment and Positioning Procedures of Seat and Dummy

- ✗ The adjustment procedures from current protocol are **not applicable** to seats with **larger angles**.
- ✗ **H-point and posture like pelvis angle** of reclined dummy is quite **different** from the current upright dummy.
- ✗ The reclined posture prediction function is only applicable when the **seat cushion angle is 14.5°**. (Reed et al. 2019 TIP)



- Adjustment procedures of other parts of the dummy are basically consistent with that of the THOR-50M dummy in MPDB test protocol of C-IASI.

## ■ Pelvis Angle and H-point of Dummy



To calculate **pelvis angle**, rotate the seat **until the seat cushion angle is 14.5°**:

- Based on the torso angle **BA<sub>SP</sub>** measured by HPM-II, **PA<sub>SP</sub>** is

$$PA_{SP} = 0.33BA_{SP} + 50.6^\circ$$

(Reference: Reed et al. 2019 TIP)

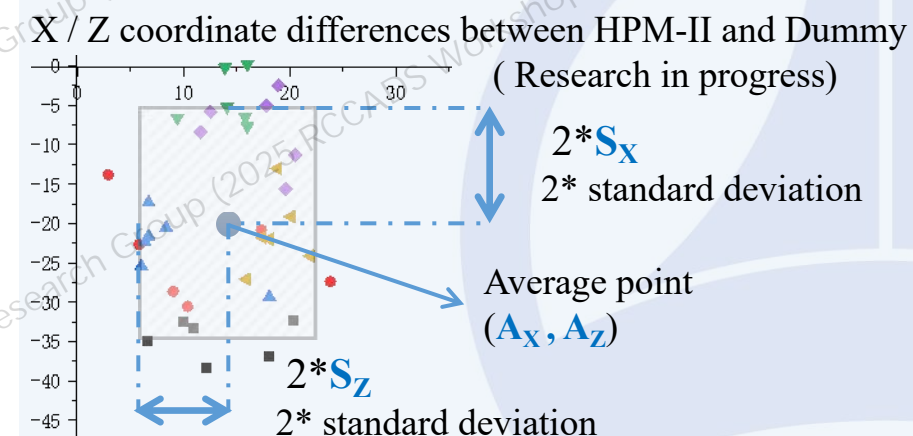
- Based on the seat rotation angle **Angle<sub>D</sub>** and the difference **X** between pelvis angle sensor values and human pelvic angles caused by different dummy structures, the target pelvic angle of dummy **PA<sub>dummyTP</sub>** is

$$PA_{TP} = PA_{SP} + Angle_D, PA_{dummyTP} = PA_{TP} + X$$

- To obtain **H-point** of the dummy, HPM-II is used for H-point, and the method of using the HPM-II refers to SAE J4002.
- The coordinate relationship between the H-point measured by the HPM-II and the H-point of the dummy should meet the following ranges:

$$X_{Dummy} = X_{HPM-II} + A_X \pm 2 * S_X \text{ mm}$$

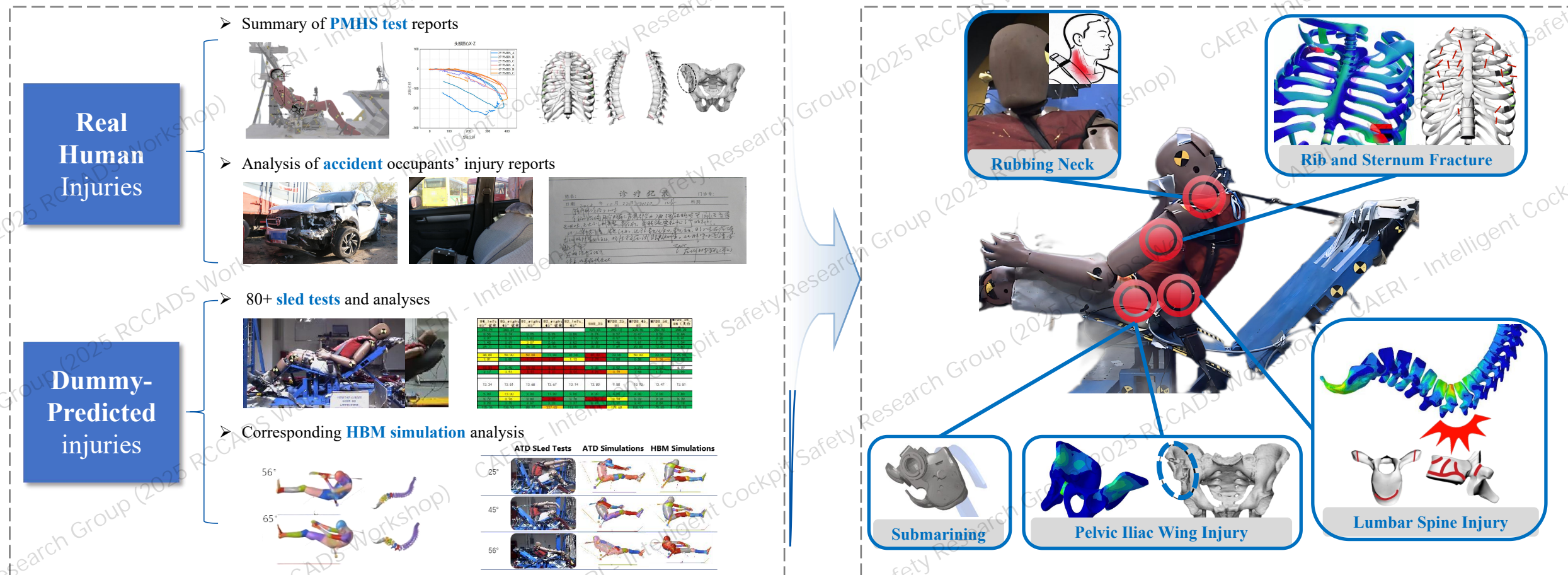
$$Z_{Dummy} = Z_{HPM-II} + A_Z \pm 2 * S_Z \text{ mm}$$





## ■ Main Risks of Reclined Occupants

❑ What are the main injury risks for reclined occupants in frontal impacts?



✓ Risks are concentrated in the **thorax**, **pelvis**, and **lumbar spine**, with kinematic risks of **submarining** and **belt rubbing neck**.

## ■ Lumbar Spine

- In **9 out of 11** frontal impact reclined cadaver tests, **AIS2+** injuries were observed in the T12 - L5 vertebrae, among which **7 of the 9** cases were **AIS3**.

- <https://www.nhtsa.gov/research/biomechanics>
- Baudrit, P., et al., Stapp Car Crash J, 2022.
- Richardson, R., et al., Stapp Car Crash J, 2020.

### □ How to assess lumbar spine injury in dummy?

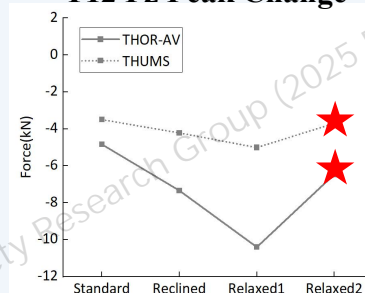
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Partial Reclined	45°	25°	\
Fully Reclined 1	56°	15°	40°
Fully Reclined 2 ★	65°	30°	30°

★ submarining

Posture	Torso Angle	Cushion Angle
Standard	25°	15°
Reclined	45°	15°
Relaxed1 ★	65°	15°

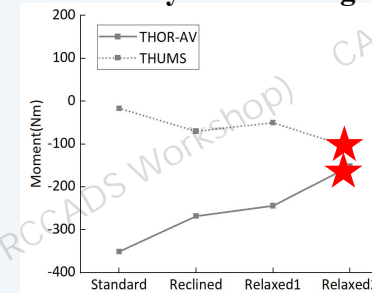
★ submarining

T12 Fz Peak Change



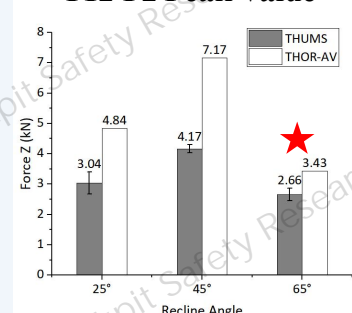
Consistency

T12 My Peak Change



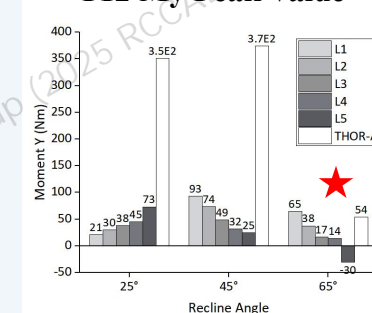
Inconsistency

T12 Fz Peak Value



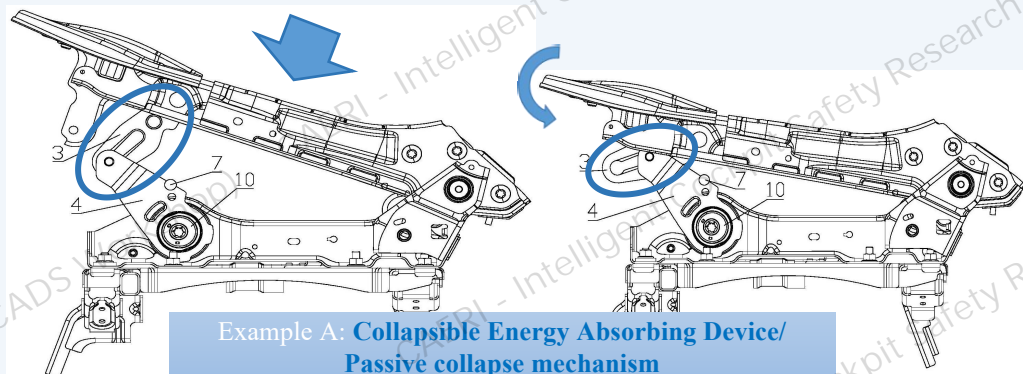
Ratio 1.6 / 1.7

T12 My Peak Value



Inconsistency

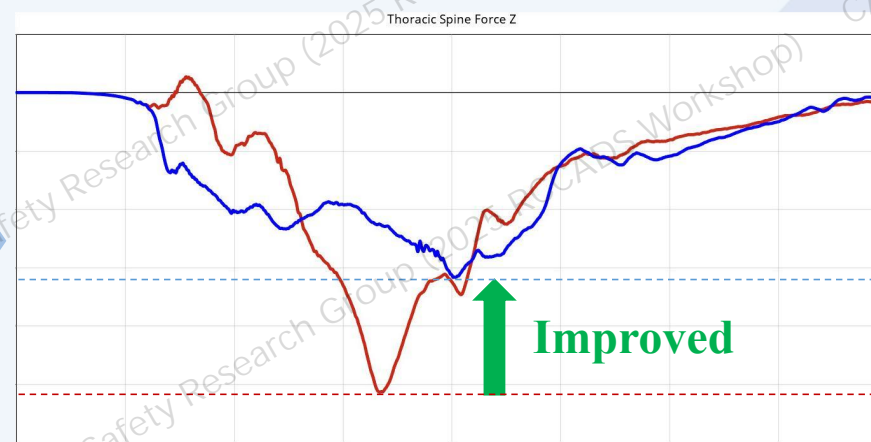
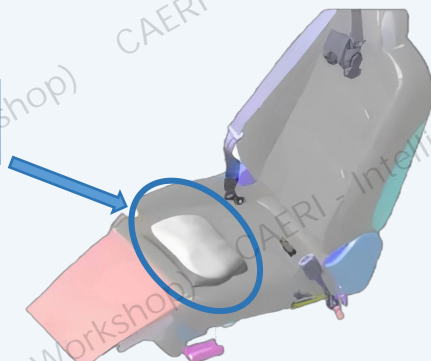
## ■ Examples of solutions for excessive lumbar axial compression force



Example A: **Collapsible Energy Absorbing Device/  
Passive collapse mechanism**  
Patent: CN221137781U



Example B: **Cushion Airbag**





## Pelvic Iliac

- In **7 out of 11** frontal impact reclined cadaver tests, **AIS2+** injuries were observed.

- <https://www.nhtsa.gov/research/biomechanics>
- Baudrit, P., et al., *Stapp Car Crash J*, 2022.
- Richardson, R., et al., *Stapp Car Crash J*, 2020.
- Moreau, D., et al., *Ann Biomed Eng*, 2023.
- Richardson, R., et al., *Traffic Inj Prev*, 2024.

Annals of Biomedical Engineering (2023) 51:1942–1949  
https://doi.org/10.1007/s10439-023-03244-8

ORIGINAL ARTICLE

BMES BIOMECHANICAL  
ENGINEERING  
SOCIETY

### Development of an Injury Risk Function for the Anterior Pelvis Under Frontal Lap Belt Loading Conditions

David Moreau<sup>1</sup> · Pavel Chernyavskiy<sup>2</sup> · Sara Sochor<sup>1</sup> · Bronislaw Gepner<sup>1</sup> · Jason Forman<sup>1</sup> · Martin Östling<sup>3</sup> · Jason R. Kerrigan<sup>1</sup> 

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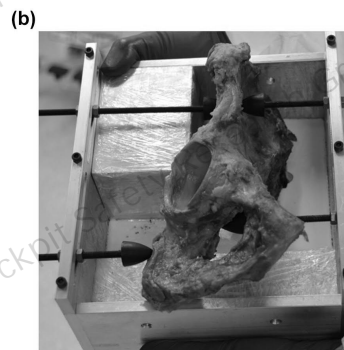
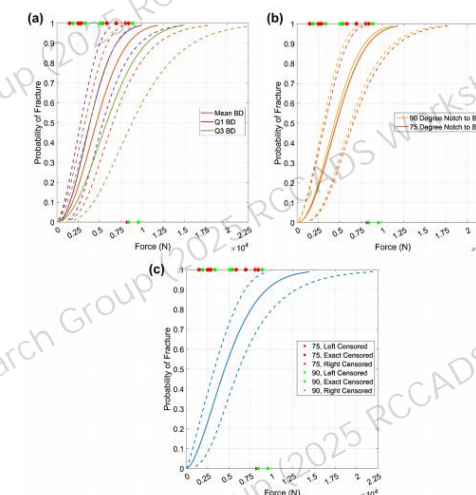


Table 3 Model parameters with goodness of fit

Model	Corrected AIC (AICc)	Shape (s)	$\beta_{\text{lower}}$ [95% CI]	$\beta_{\text{up}}$ [95% CI]	$\beta_{\text{shape}}$ [95% CI]	Injury Risk Function P(Fracture   Force)
Base	328.6	1.619	8.637 [8.350, 8.923]	—	—	$1 - e^{-e^{(Force/8.637)^{1.619}}}$
BD	324.5	2.016	—0.570 [−5.814, 4.674]	6.854 [2.924, 10.783]	—	$1 - e^{-e^{(Force/6.854)^{2.016}}}$
Angle	331.1	1.627	8.696 [8.288, 9.103]	—	−.117 [−.676, .442]	$1 - e^{-e^{(Force/8.696)^{1.627}}}$
Angle and BD	327.5	2.020	−0.859 [−6.687, 4.970]	7.048 [2.760, 11.334]	0.057 [−.434, .547]	$1 - e^{-e^{(Force/7.048)^{2.020}}}$



Pelvic Iliac Wing  
Injury Risk Function

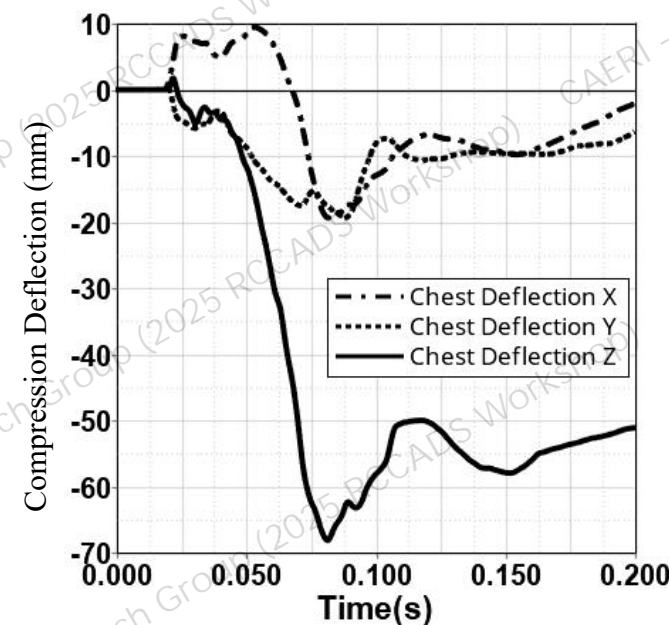
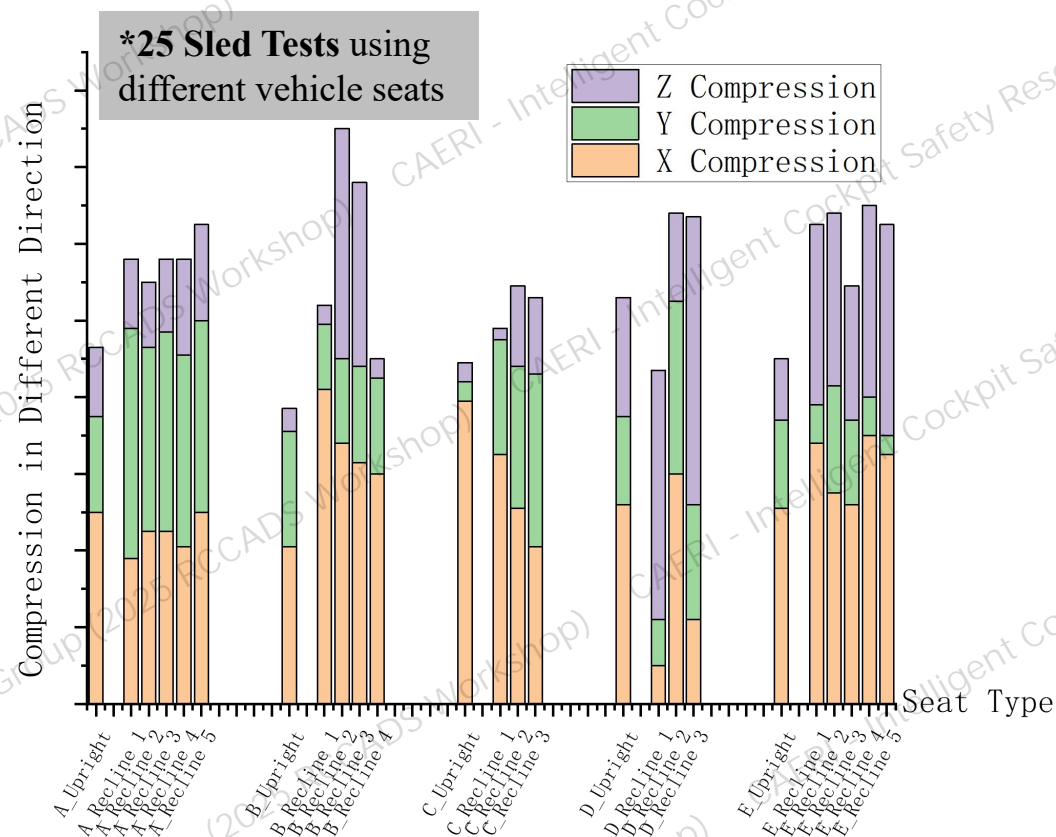
□ A dummy only has force sensors in X direction **F<sub>x</sub>** for iliac wing now.

□ How to assess pelvic iliac injury in dummy?



## ■ Thorax Injury

- ❑ In reclined posture, almost every cadaver test resulted in **rib or sternum fractures**.
- ❑ In reclined posture, ATD tests and simulations indicate that the **chest compression deformation** will be **higher** and the **Z direction** of chest compression **may contribute more**.



Rating	Good	Acceptable	Marginal	Poor
Chest Compression Deformation (mm)	Monitor (X/Y/Z and Resultant)			

## ■ Abdomen Injury

❑ If the occupant **submarines**, the belt force acting directly on the abdomen may cause organ damage.

### Dummy Abdominal Pressure

### Dummy Abdominal Compression Deformation

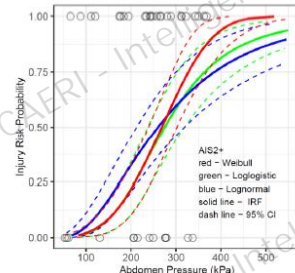


Figure 14. Abdomen MAIS2+ injury risk curves

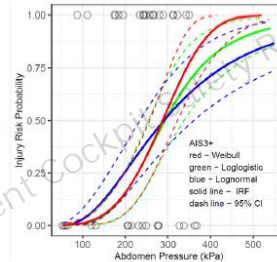


Figure 15. Abdomen MAIS3+ injury risk curves

Table 8. Abdomen pressure injury risk function scale and shape parameters and injury risk values

AIS	Fit	Shape	Scale	AIC	GKG	AUROC	Qual. Index	Injury Risk Values (kPa)		
								5%	25%	50%
MAIS2+	Weibull	3.5054	298.5578	312.8	0.19	0.597	0.23	128	209	269
	Loglogistic	3.9430	275.2554	322.6	0.11	0.557	0.30	130	208	275
	Lognormal	1.7177	260.3630	344.1	0.07	0.536	0.40	100	176	260
MAIS3+	Weibull	3.8799	316.2339	255.6	0.16	0.579	0.23	147	229	288
	Loglogistic	4.4597	293.2402	261.3	0.10	0.550	0.28	152	229	293
	Lognormal	1.7547	290.5577	285.0	0.05	0.524	0.43	114	198	291

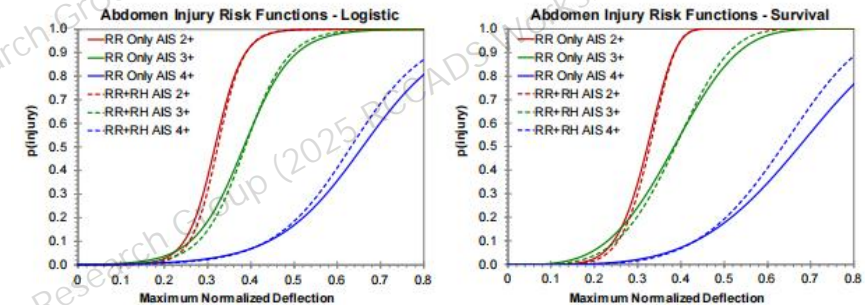
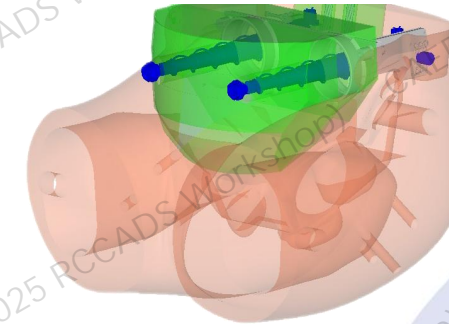


Figure 6.8. Abdomen injury risk functions calculated using AIS 2+, 3+, and 4+ as the injury definition.



Restraint System and ATD Kinematic						
Derived from restraint system and ATD kinematic demerits				Demerits		
1.1.1	Head and Neck Protection					
1.1.1.1	Dangerous deployment of frontal airbag <sup>1</sup>			1		
1.1.1.2	Diagonal belt slippage (obvious rubbing with ATD's neck)			1		
1.1.1.3	Two or more hard contacts on the head <sup>2</sup>			1		
1.1.2	Chest and Abdomen Protection					
1.1.2.1	Excessive shoulder belt load (6kN)			2		
1.1.3	Knee and Pelvis Protection					
1.1.3.1	ATD submarining			4		
1.1.4	Other Protection					
1.1.4.1	Failure to unlock the seat belt or excessive unlocking force <sup>3</sup>			1		
1.1.4.2	Seat Failure (Do NOT include seat failures resulting from design for the purpose of achieving occupant protection)			6		
Restraint System and ATD Kinematics Rating			Good	Acceptable	Marginal	Poor
Demerits			≤1	≤3	≤5	≥6

3. Failure to unlock the seat belt or excessive unlocking force (1 defect) means that when the dummy is released from the restraint system after a collision, the seat belt cannot be unlocked or the unlocking force of the seat belt buckle is greater than 60N.



## ■ ATD Injury Rating

ATD Injury					
2.1	ATD Injury Rating				
2.1.1	Head/Neck	Good	Acceptable	Marginal	Poor
2.1.1.1	HIC15	≤560	≤700	≤840	>840
2.1.1.2	Shear Force F <sub>x</sub> (kN) ※	≤1.9	≤2.5	≤3.1	>3.1
2.1.1.3	Tensile Force F <sub>z</sub> (kN) ※	≤2.7	≤3.0	≤3.3	>3.3
2.1.1.4	Tensile Bending Moment M <sub>oc</sub> (Nm) ※	≤42	≤49.5	≤57	>57
If there is one hard contact resulting in the resultant head acceleration exceeding 70 g, the head and neck injury rating will be degraded by one level, but the defects in the restraint system and ATD kinematics rating will not be counted					
2.1.2	Chest/Abdomen	Good	Acceptable	Marginal	Poor
2.1.2.1	Chest Compression Deformation (mm)	Monitoring(X/Y/Z and Resultant)			
2.1.2.2	Abdomen Pressure (bar)	≤1.28	≤2.09	≤2.69	>2.69
(Depends on dummy)	Abdomen Compression Deformation (mm)	Monitoring(X/Y/Z and Resultant)			
2.1.3	Thigh/Hip	Good	Acceptable	Marginal	Poor
2.1.3.1	Compression Force on Thigh F <sub>z</sub> (kN)	≤3.8@0ms ≤3.8@10ms	≤6.44@0ms ≤5.68@10ms	≤9.07@0ms ≤7.56@10ms	>9.07@0ms >7.56@10ms
2.1.3.2	Compression Force on Acetabulum F <sub>AR</sub> (kN)	≤3.28	≤3.69	≤4.1	>4.1
2.1.3.3	Iliac Force F <sub>x</sub> (kN)	≤2.5	≤3.5	≤4.5	>4.5
2.1.3.4	Lap Belt Force (kN)	Monitoring			
2.1.4	Spine	Good	Acceptable	Marginal	Poor
2.1.4.1	Lumbar Spine Compression Force T12 F <sub>z</sub> (kN)	≤4.5	≤5.5	≤6.5	>6.5
2.1.4.2	Lumbar Spine Bending Moment T12 M <sub>y</sub> (Nm)	Monitoring			
2.1.5	Tibia/Foot	Good	Acceptable	Marginal	Poor
2.1.5.1	Knee joint sliding displacement D (mm)	≤12	≤15	≤18	>18
2.1.5.2	Tibia index (upper and lower) TI	≤0.8	≤1.0	≤1.2	>1.2
2.1.5.3	Tibia axial force F <sub>z</sub> (kN)	≤4.0	≤6.0	≤8.0	>8.0
2.2.5.4	Maximum resultant foot acceleration A(g)	≤150	≤200	≤260	>260

Neck※ -- The current neck criteria and thresholds are derived from the THOR dummy in the current C-IASI protocols, and may be updated based on research.



## Overall Rating and Protocol Location

- Physical tests. C-IASI → Vehicle Occupant Safety Index → Additional Protocols **(TBD)** ;
- Select the lowest-configured vehicle equipped with reclined seats for testing. Each position with a reclined seat (eg. the front-passenger seat, second-row seats) needs to be tested separately. Then, pick the worst result among all.

Rating Object	Overall Rating			
	GOOD (G)	ACCEPTABLE (A)	MARGINAL (M)	POOR (P)
Driver/front-passenger/second-row, etc.	Pick the worst rating			
Head and Neck	0	2	10	20
Chest and Abdomen	0	2	10	20
Thigh and Hip	0	2	10	20
Spine	0	2	10	20
Leg and Foot	0	1	2	4
Restraint System and ATD Kinematic	0	2	6	10
Overall Rating Cutoffs	0-3	4-9	10-19	20+

## Sample Provision



JOYSONELECTRONICS

ADIENT

## Simulation and Analysis



BYD



## Comparative Analysis of HBMs vs ATDs & Laboratory Test Implementation



Autoliv



## Injury Criteria and Thresholds Research



## Protocol Feedback



ADIENT

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Background

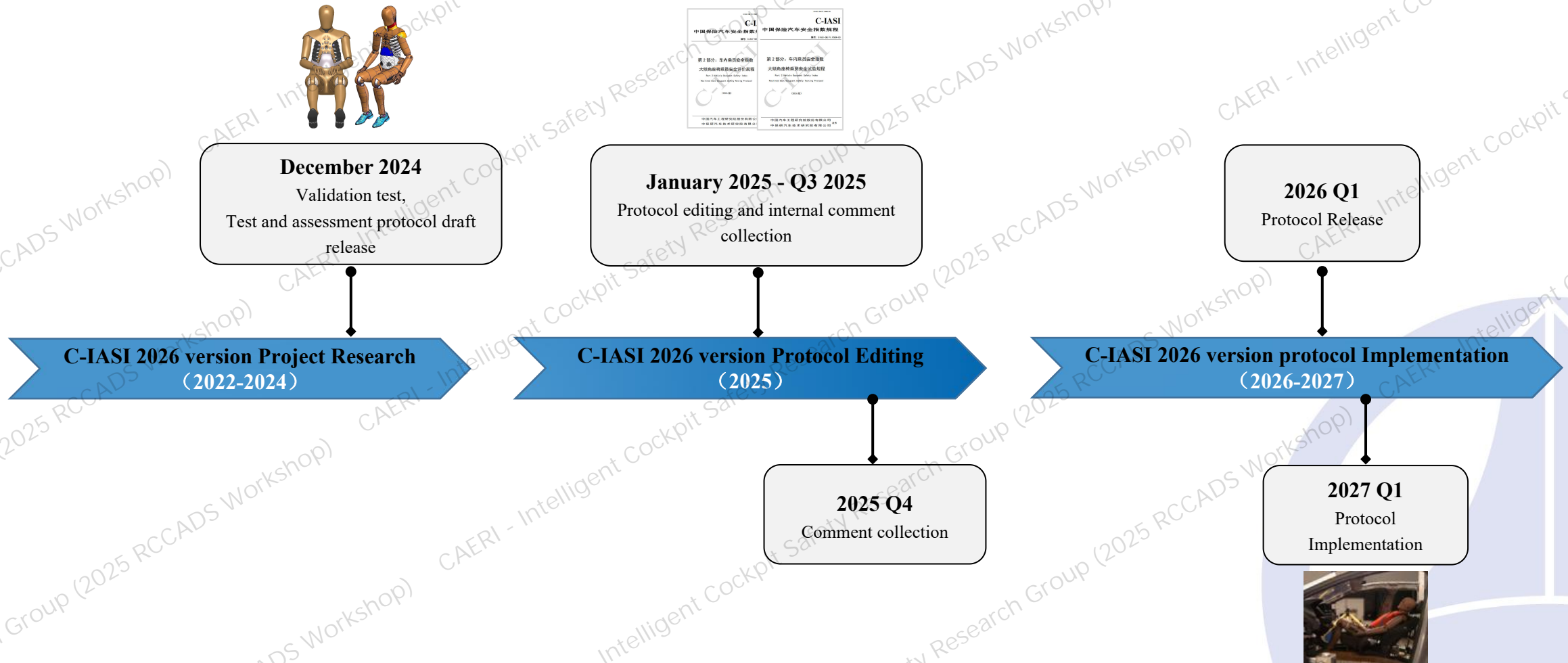
2

Research and Draft Protocol

3

Future Work

# 3.1 Protocol Plan







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